

Seeing the Options: Challenges and Strategies in Developing IVRT Methods for Ophthalmic Products

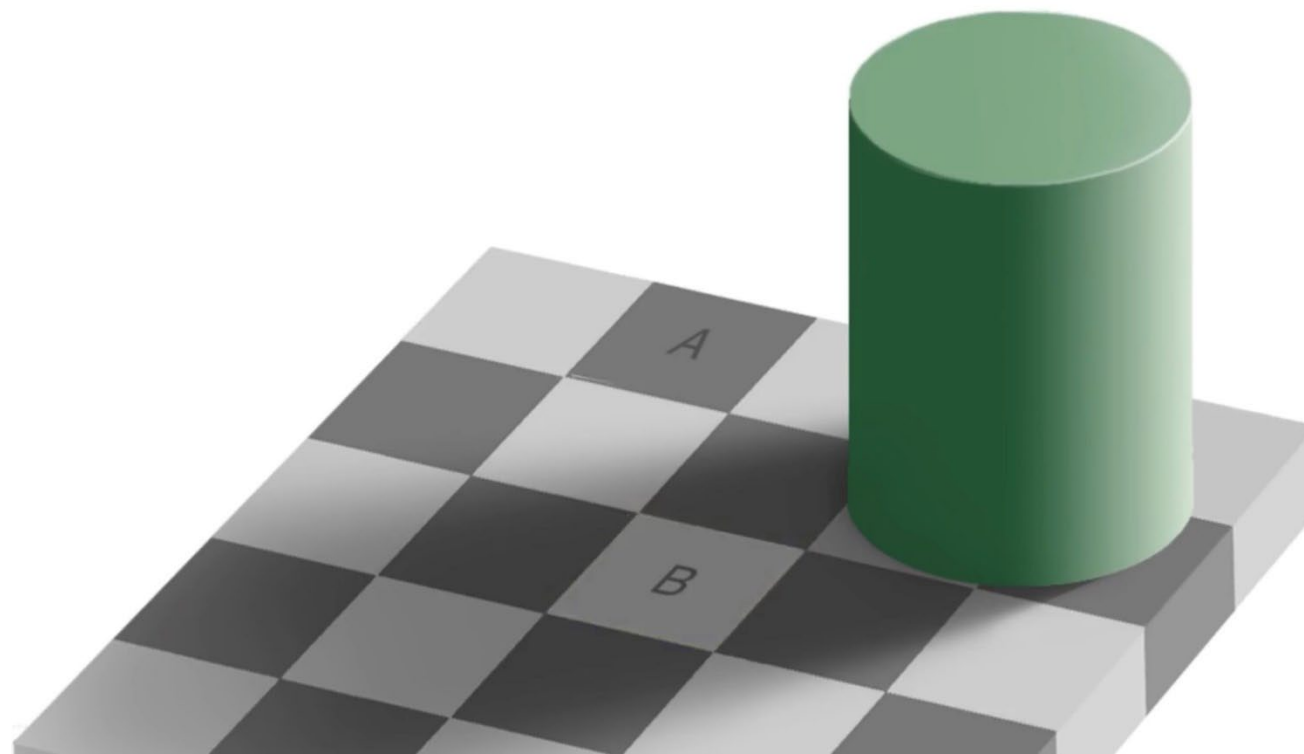
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Perception Dilemma

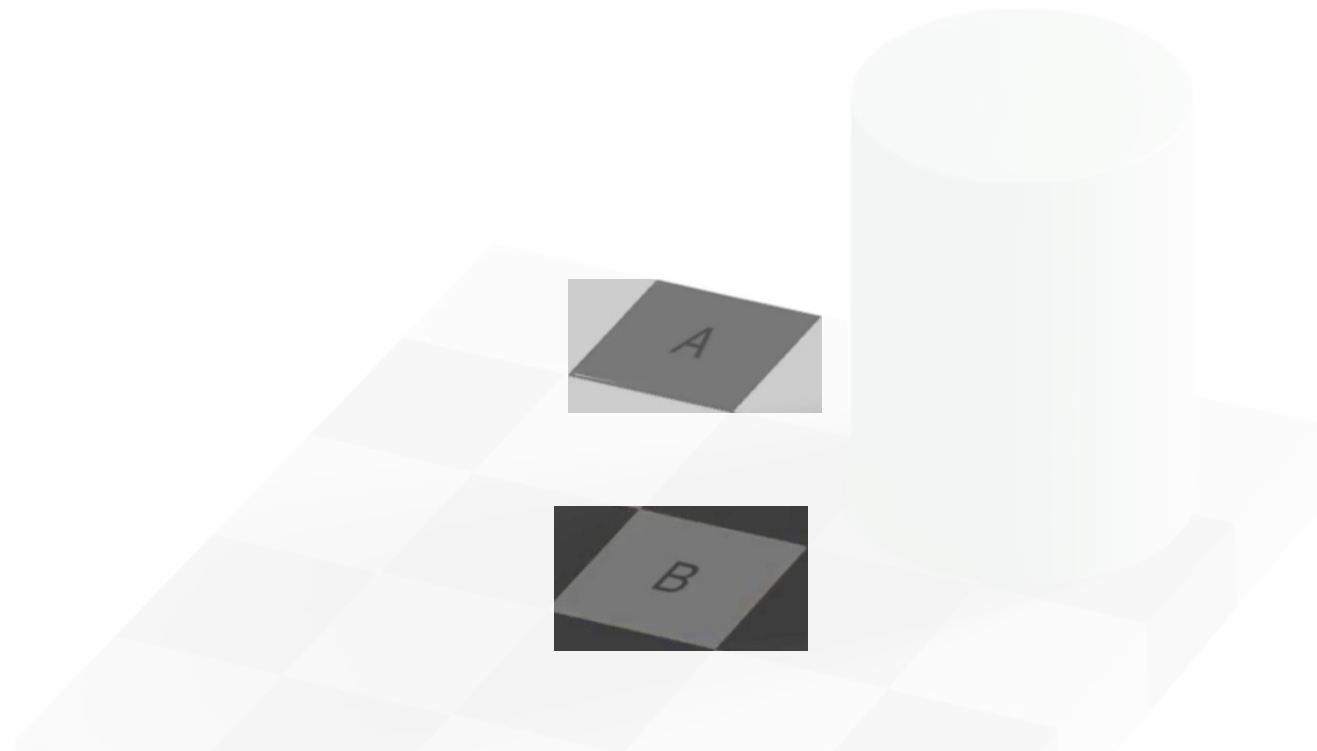


Is *A* the same as *B*?

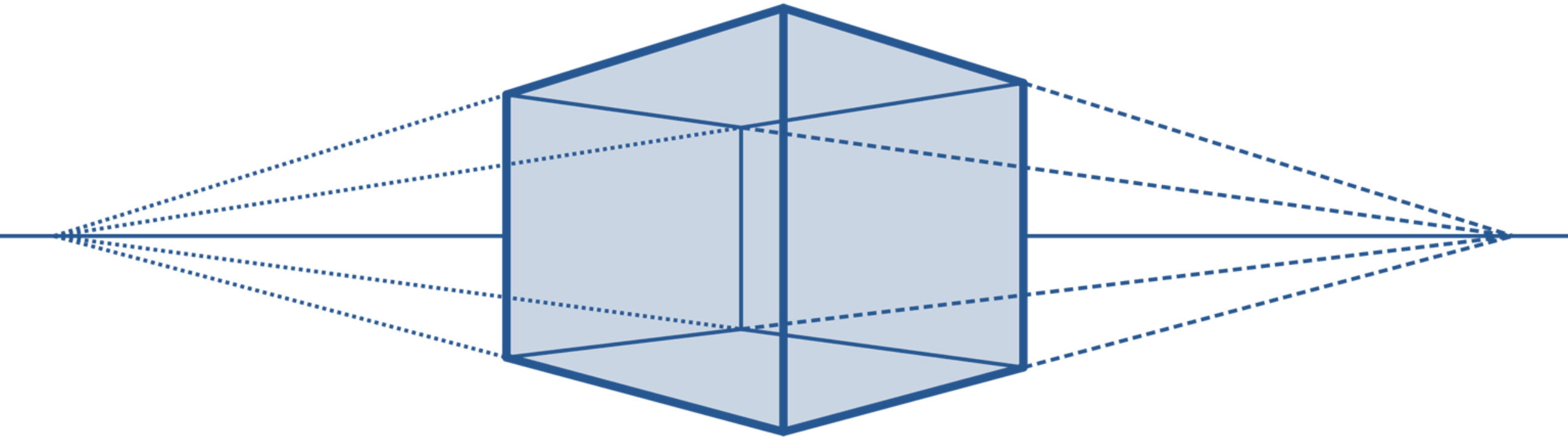


Perception Dilemma

Is *A* the same as *B*?



Perspective Limitation



Purpose of an IVRT: The Why

- Product development (formulation screening, product understanding)
- Quality control (batch-to-batch consistency)
- Bioequivalence (sameness)
- In lieu of in vivo test (IVIVC, Post-approval supplements)

Challenges in IVRT for Complex Ophthalmics



- Variable release characteristics, depending on dosage form
- Generally, lack of understanding in drug release mechanism
- The need to separate the particles from “released” drug
- Physiological constraints such as short ocular residence time, contrasting long IVRT duration
- Challenging to demonstrate the method is discriminative (against formulation and process changes)

A Good IVRT is:

Reproducible

and

Discriminatory

Precise

e.g., low CV%

Robust

e.g., against minor
disturbance to
method

Sensitive

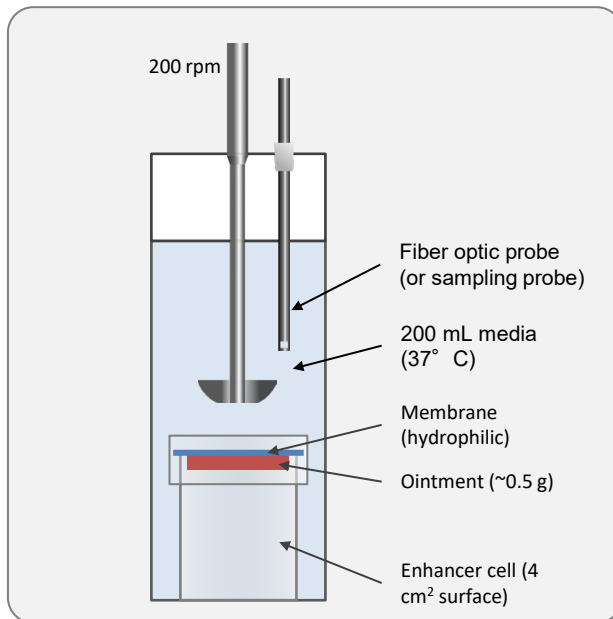
e.g., known changes in
quantity like sample with
25%, 50%, 100% drug
loading

Selective

e.g., able to detect
differences in sample
if CQAs changed,
such as particle size

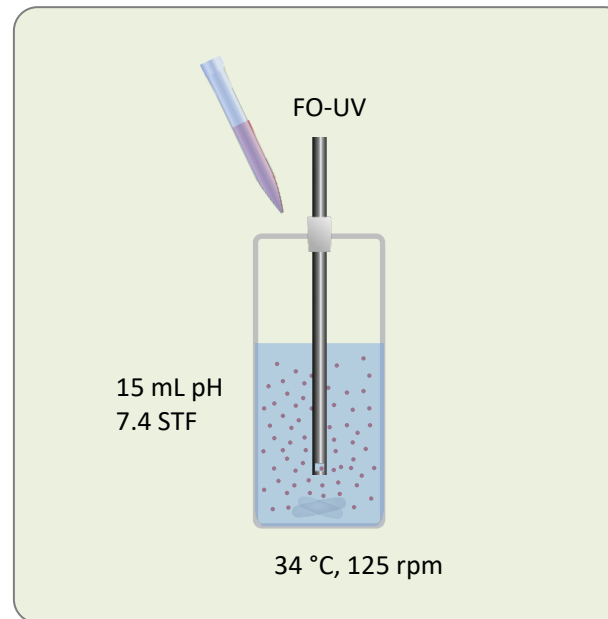
Three Examples

Ointment



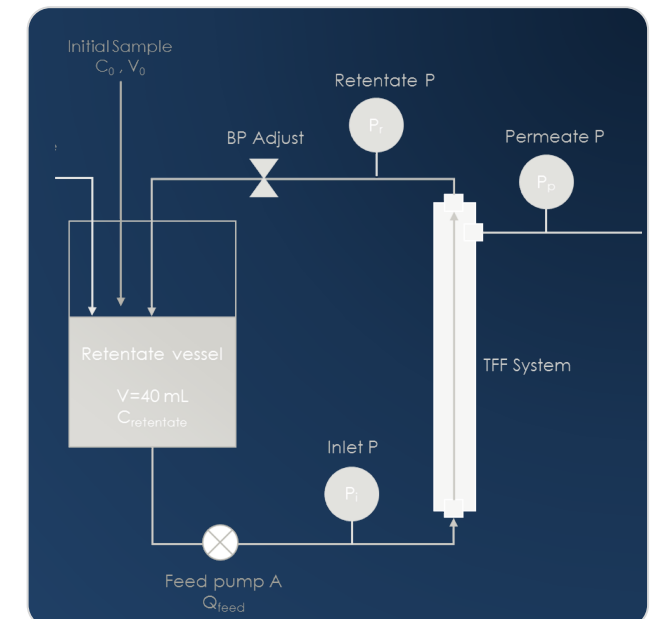
- Long release duration (hours)
- Compendial setups available (common)
- **A new kinetics theories** (Transient-Boundary vs. Higuchi)

Suspension



- Rapid release (under sink-condition) or
- Slow release when membrane separation technique is used (e.g., dialysis)
- Developed **Non-sink condition method** to capture rapid release (within seconds) and achieve discriminatory power

Emulsion

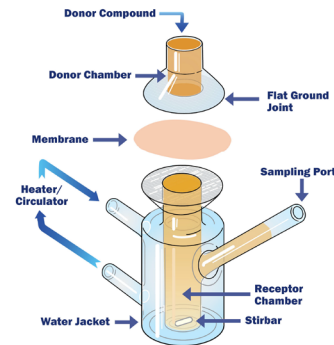


- Most complex (multiphasic: rapid and slow components)
- Membrane separation is almost always used but has severe limitations
- Developed **New method** to capture the multiphasic behavior (however, may be years away from usage)

Example 1: Ointments



Vertical diffusion cell (VDC) A,B,C



Immersion cell

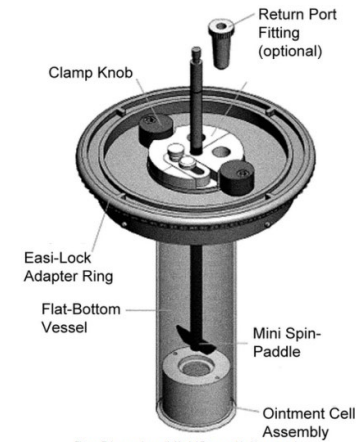


Figure 7. Immersion cell-Model B assembled in a vessel.

USP 4 with semisolid cell

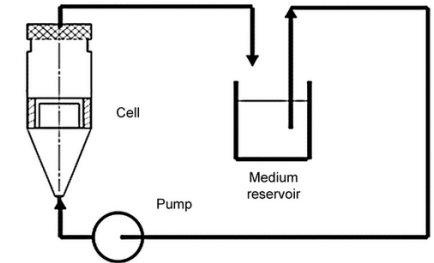
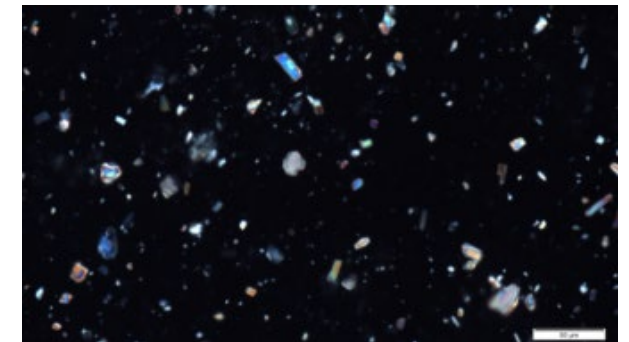
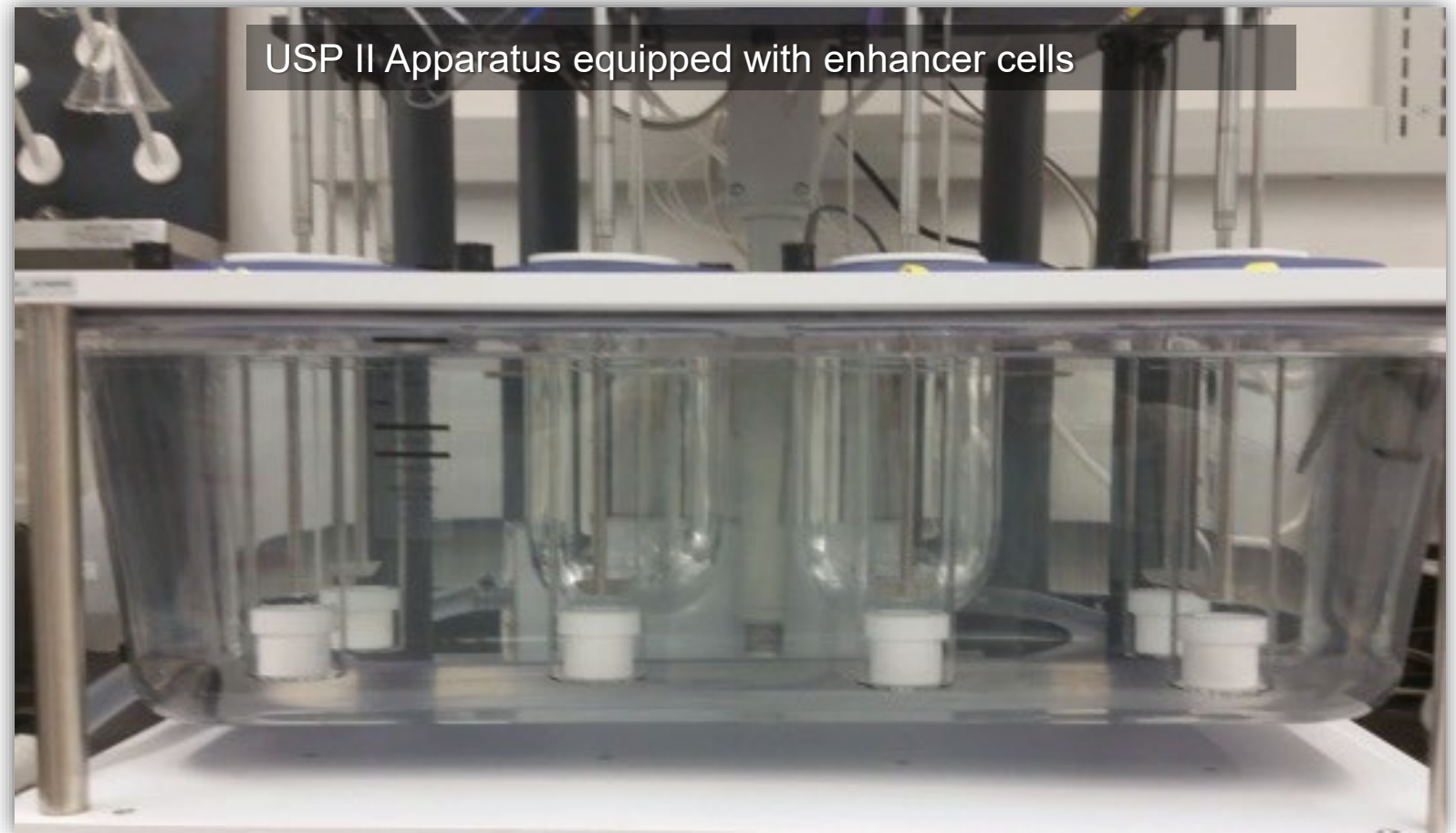
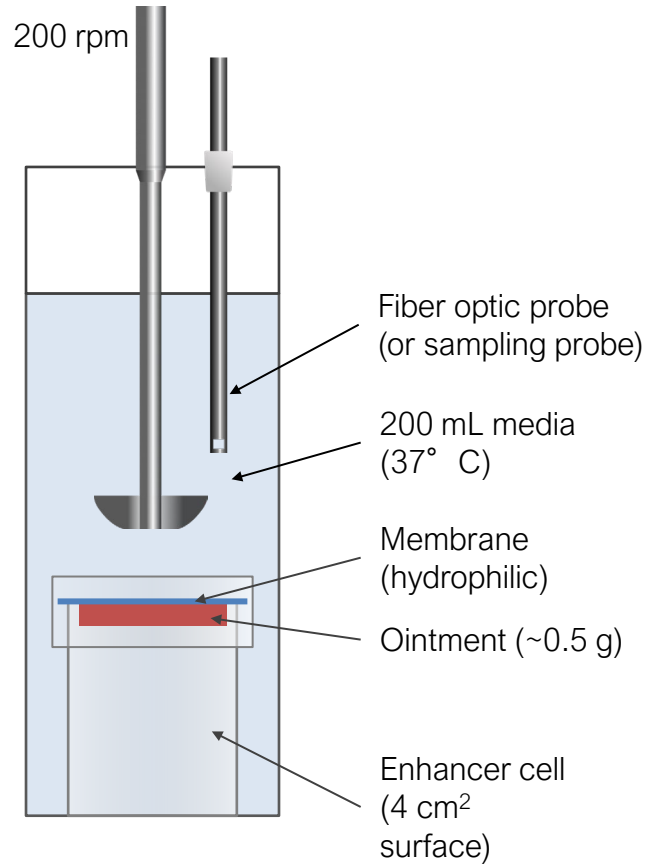


Figure 10. Closed system configuration.

- Acyclovir ophthalmic ointment, prepared in-house
- Oleaginous base (i.e., only petrolatum)
- Acyclovir remains as solid particles (not soluble in petrolatum)
- Three setups recommended by USP (for semisolids)
- Recommend to fit Higuchi release, and using T/R ratio to compare reference and test product (8th and 29th percentile)

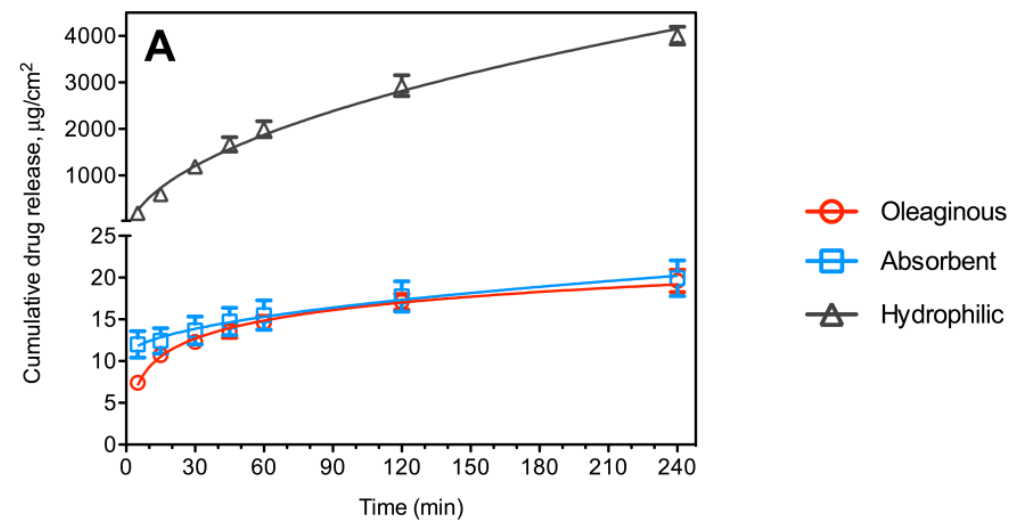


IVRT for Ointments Using Immersion Cells

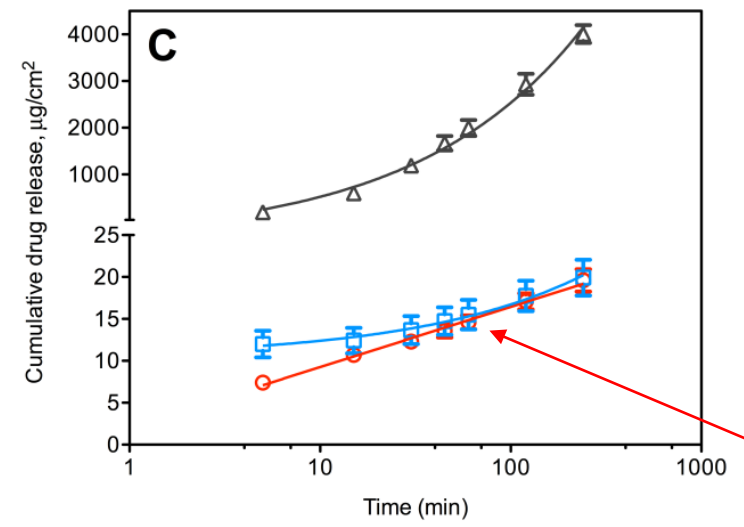
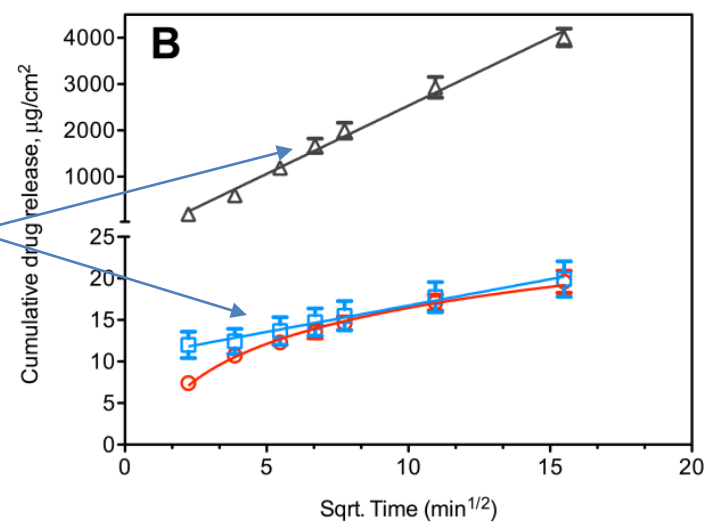


Acyclovir Release From Three Types of Ointment Bases

(A) Cumulative drug release per unit area in linear time scale; (B) Cumulative drug release per unit area plotted against square-root of time; and (C) Cumulative drug release per unit area in logarithm-time scale. (4% w/w drug loading, pH 7.4 PBS, 37° C, n=6)

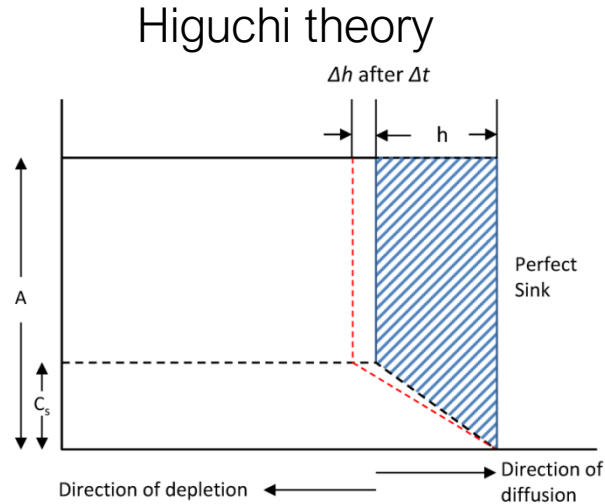


Higuchi release



Logarithm-time! Why ???

A New Transient-Boundary Layer (TBL) Theory



Inward moving boundary

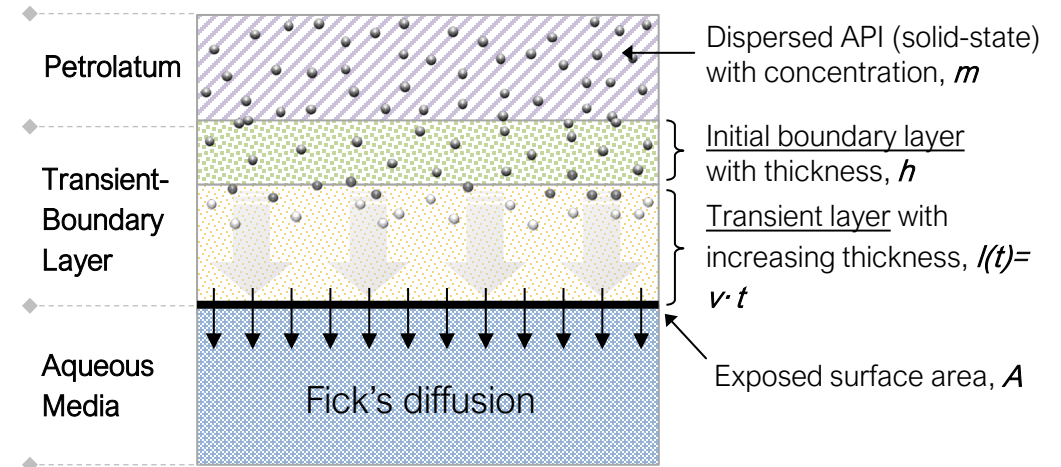
$$\frac{dQ}{dt} = \frac{D(C - C')}{h}$$

$$\frac{dQ}{dh} = A - \frac{C_s}{2}$$

$$Q_{aq} \propto \sqrt{t}$$

VS.

TBL theory



Outward expanding boundary

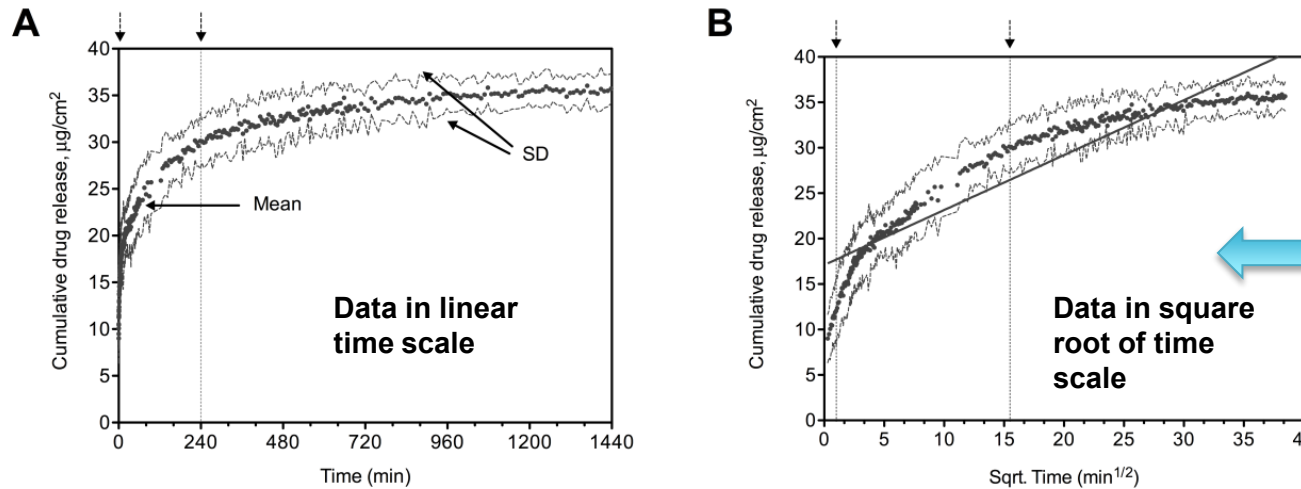
$$\frac{dQ_{aq}}{dt} = K \cdot \frac{1}{t}$$

$$Q_{aq} = K \cdot \ln(t) + Q'$$

where $K = \frac{P \cdot m \cdot h \cdot A}{v}$

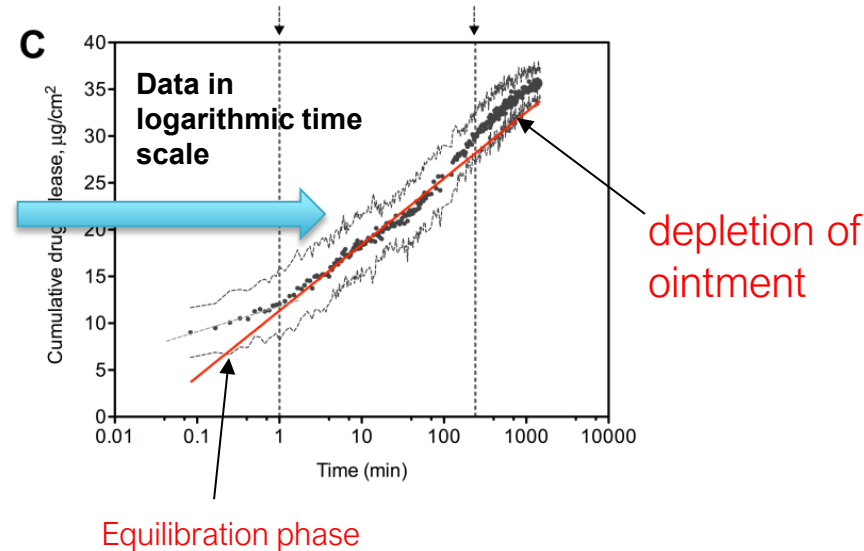
$$Q_{aq} \propto \ln(t)$$

Evidence of Logarithmic-time Dependent Drug Release



Does not follow Higuchi square-root time law

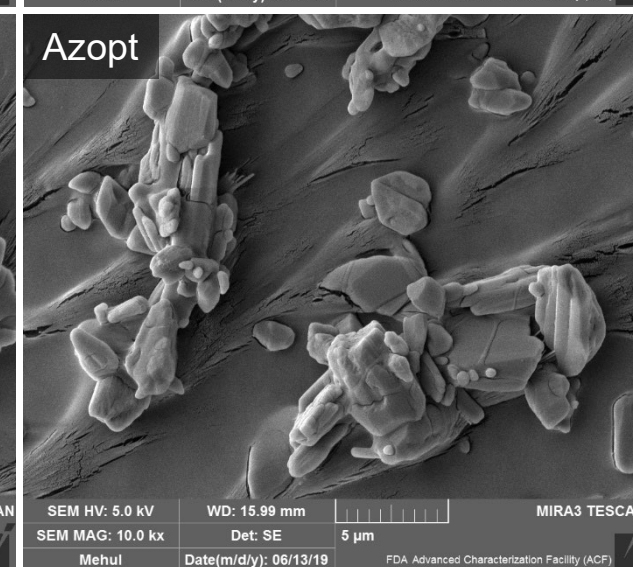
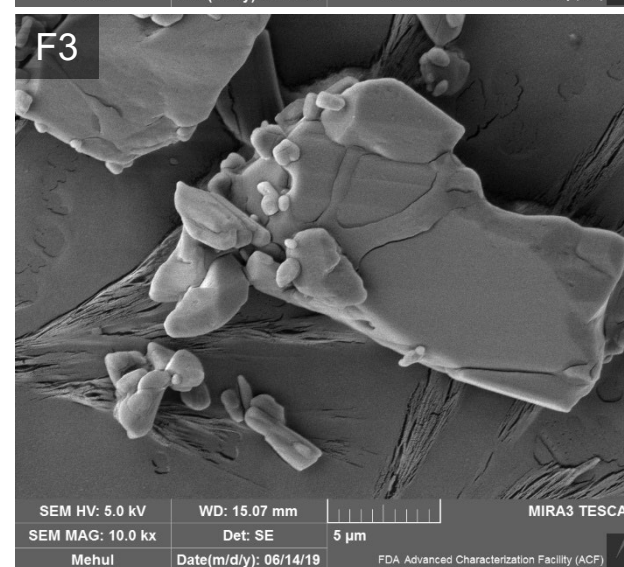
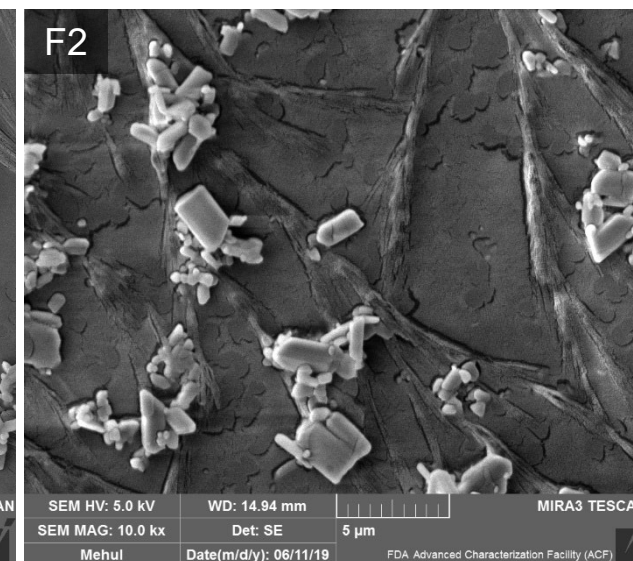
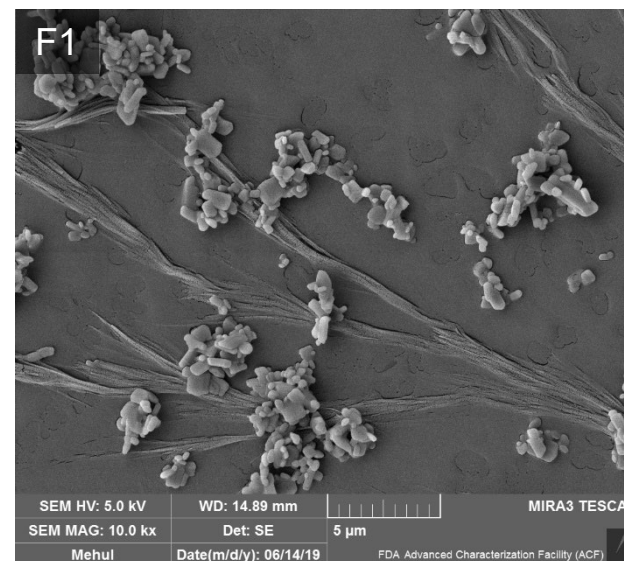
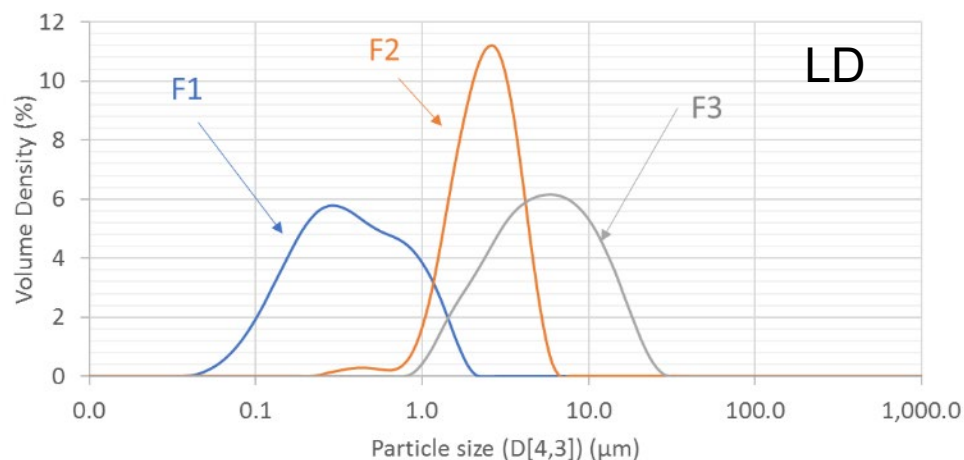
Follows Logarithmic-time scale



Example 2: Suspensions



- Brinzolamide ophthalmic suspensions
- Prepared in-house with varying PSDs (relative to the RLD)
- Expected to have different dissolution rates
- It is desired that IVRT to be discriminatory in terms of PSD, possibly supporting in vitro BE approach

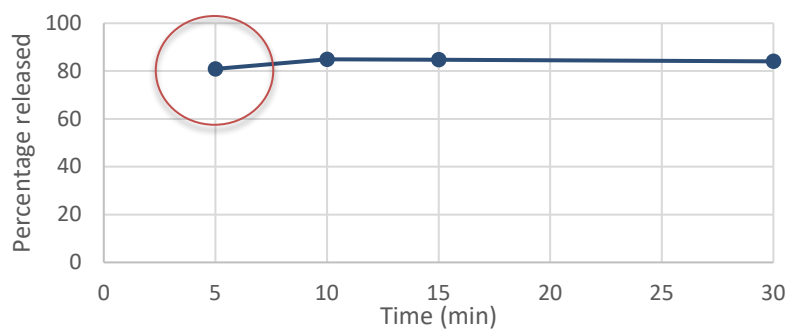
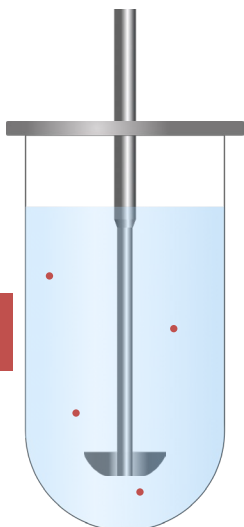


How to improve discrimination?



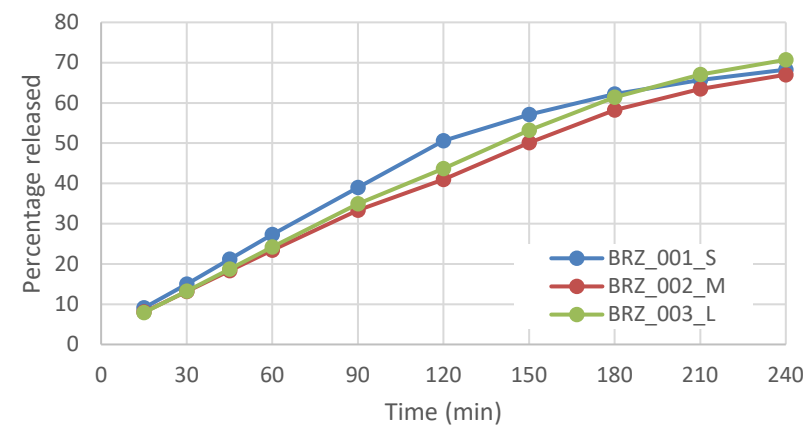
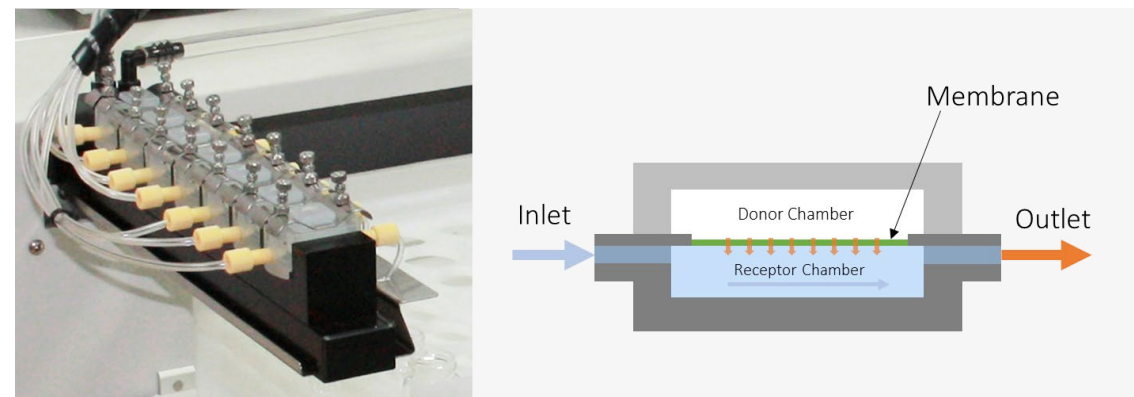
Option 1: USP 2 (900 mL)

Sink-condition!



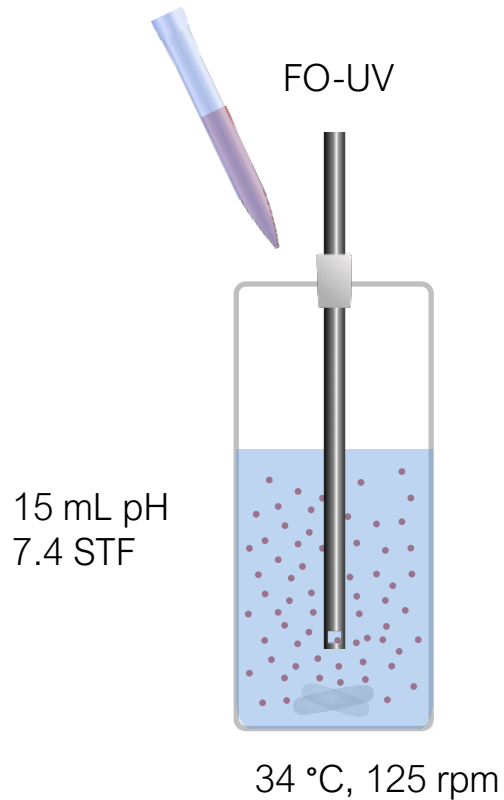
Release too fast, all formulation dissolves nearly identically

Option 2: VDC (0.45 um membrane)

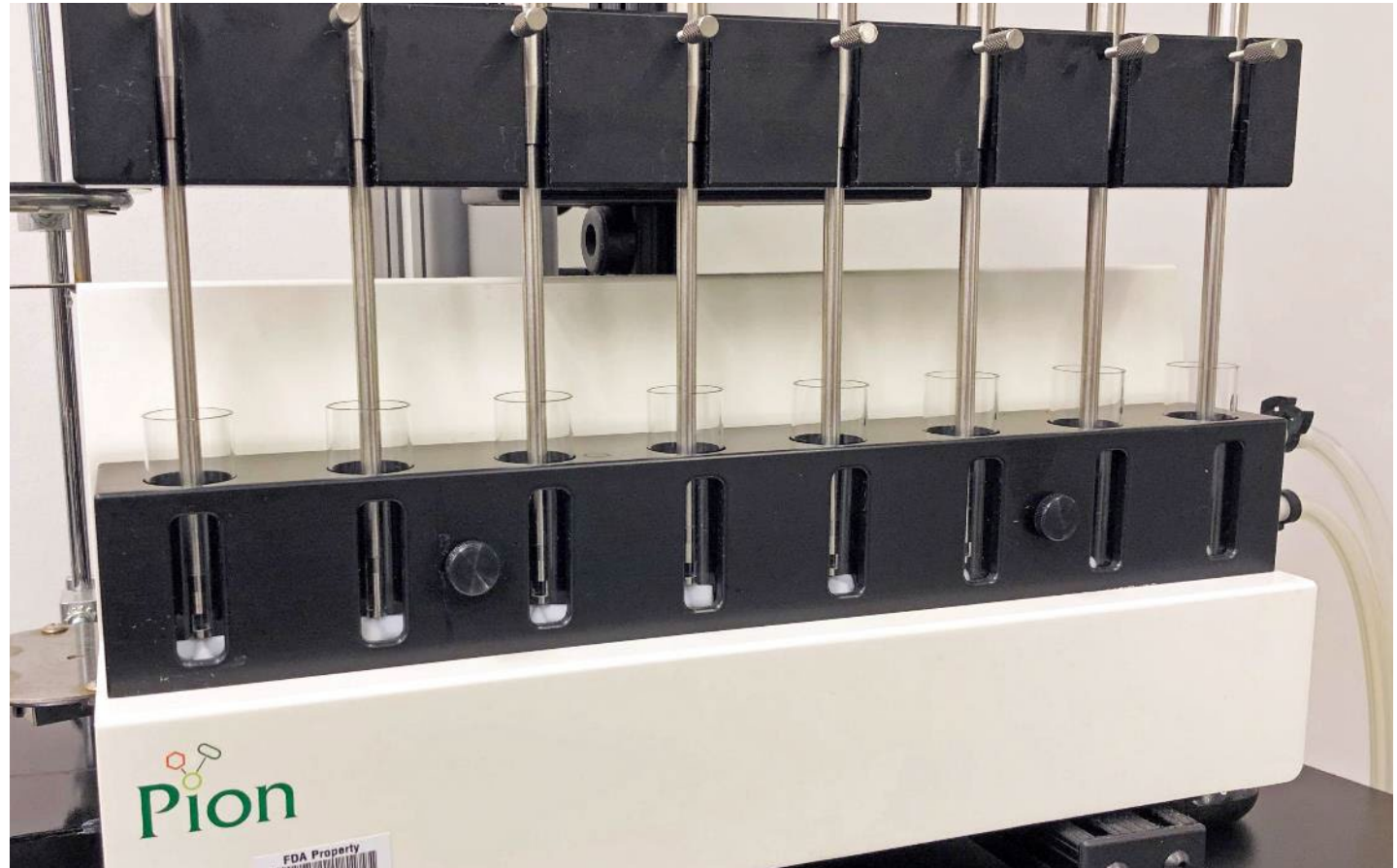


Release slowed down (by membrane), but no discrimination

How to improve discrimination? (cont.)

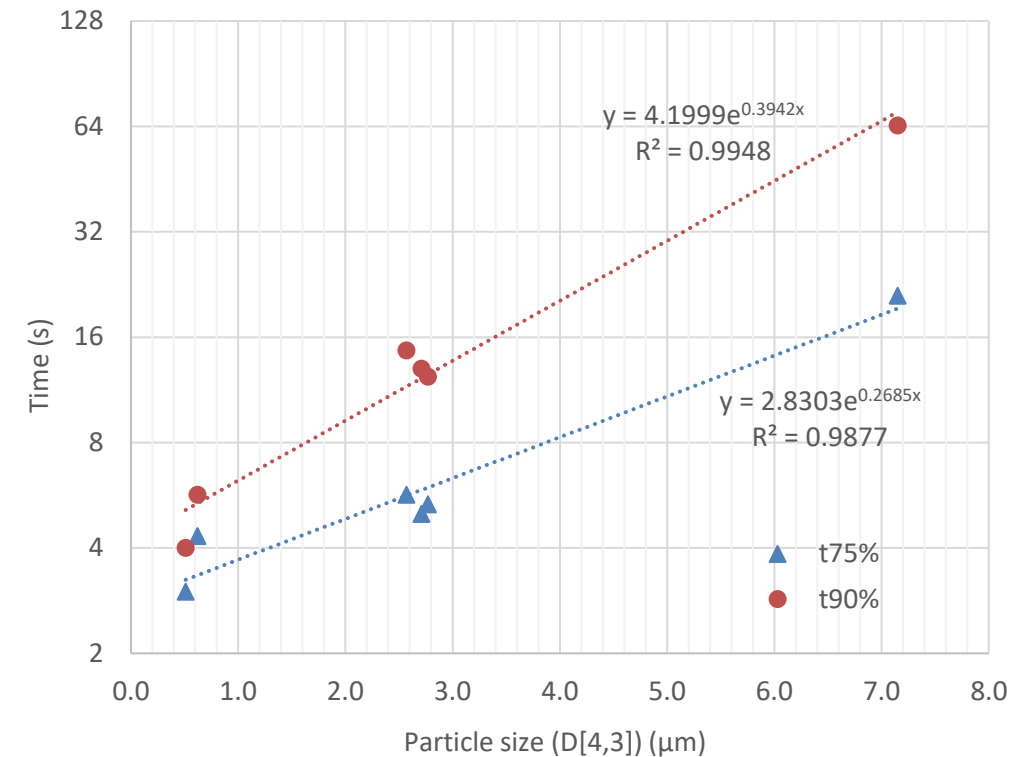
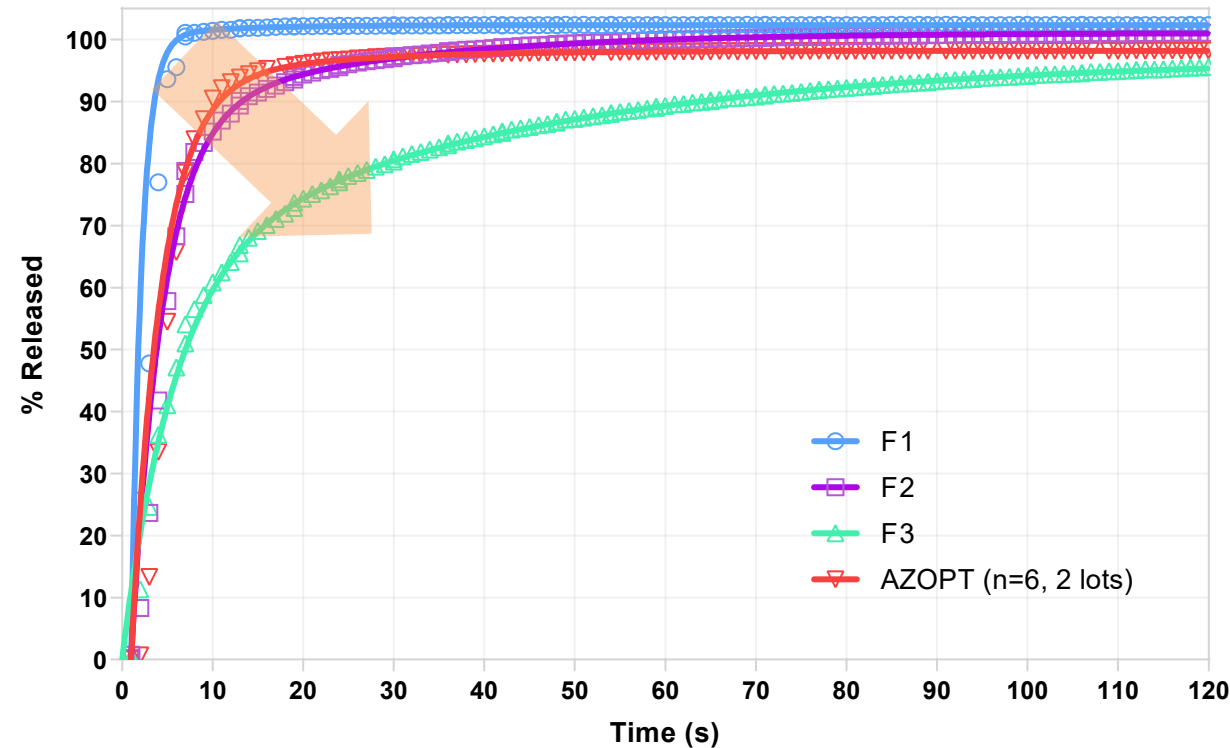


1 non-sink condition
(just like in the eye)



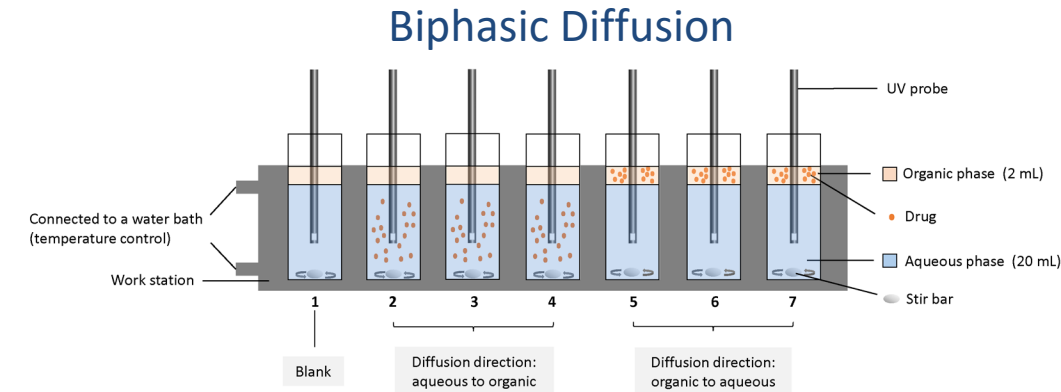
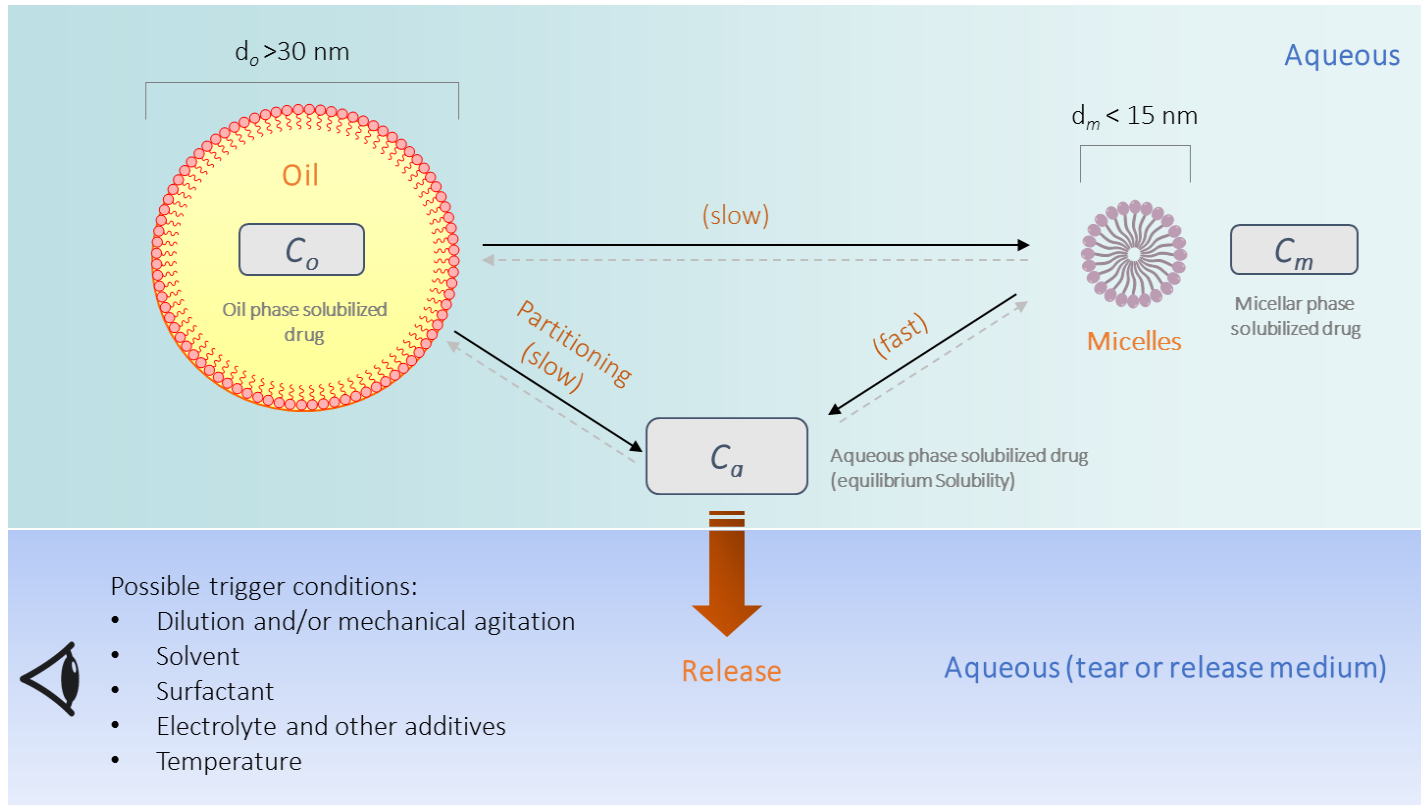
2 Continuous monitoring

Discriminatory IVRT for Suspensions



- Nano- suspensions completes dissolution within 6 seconds
- Micron- suspensions dissolves in 2 min
- Good correlation ($r^2 > 0.9$) between dissolution rate and the PSD

Example 3: Emulsions



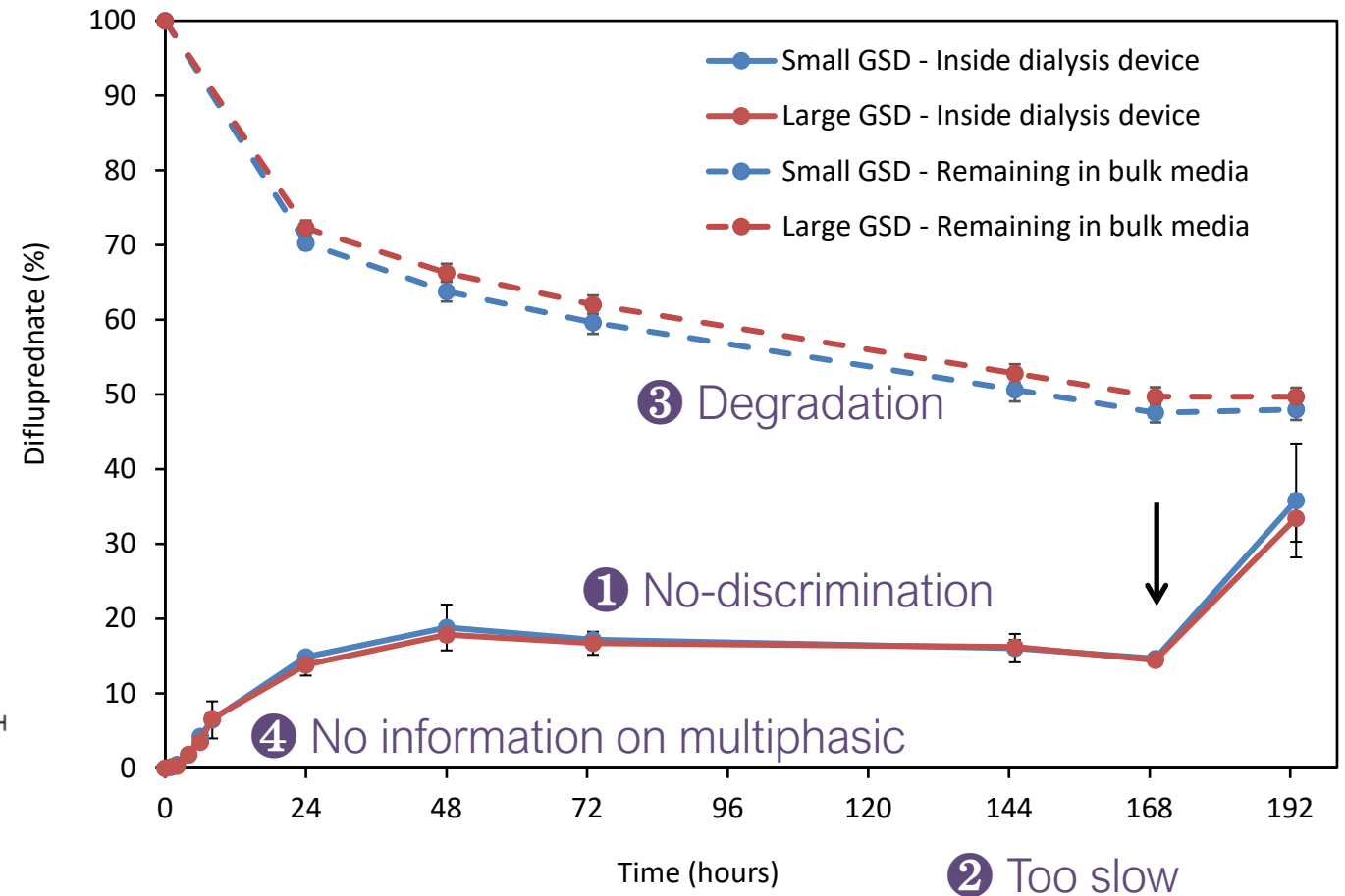
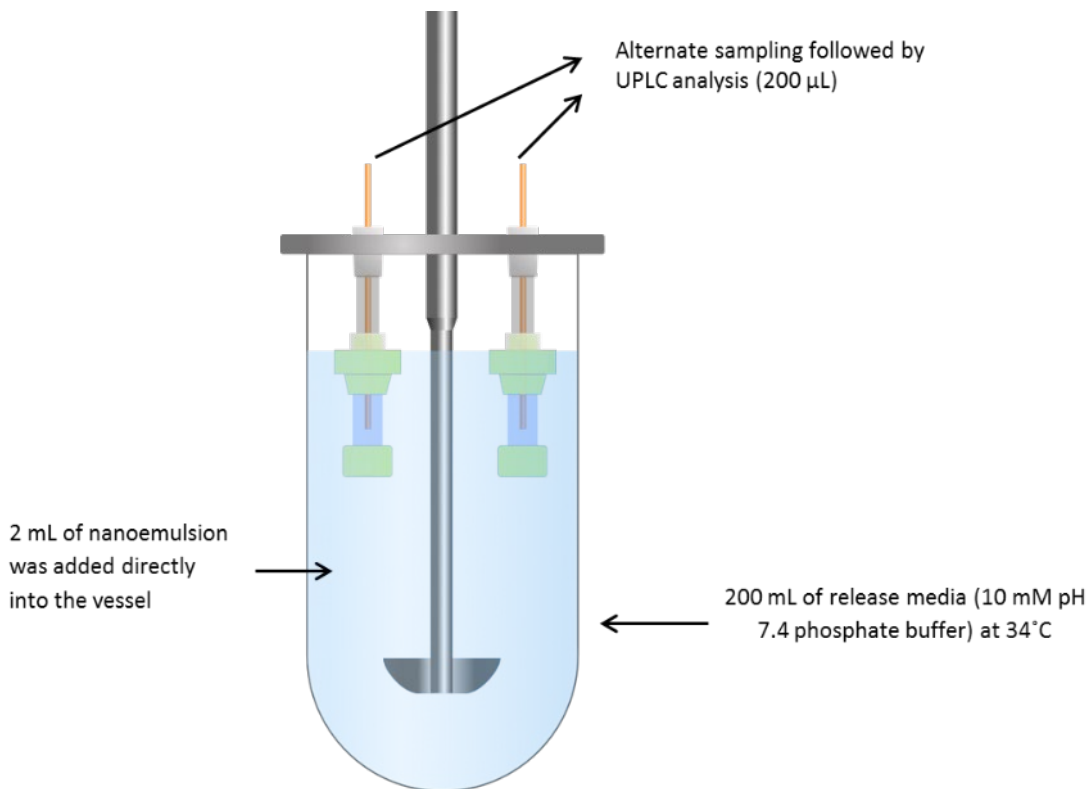
$t_{1/2}$ is approximately 12 min

Q: How to separate the released drug (at the relevant time scale)?

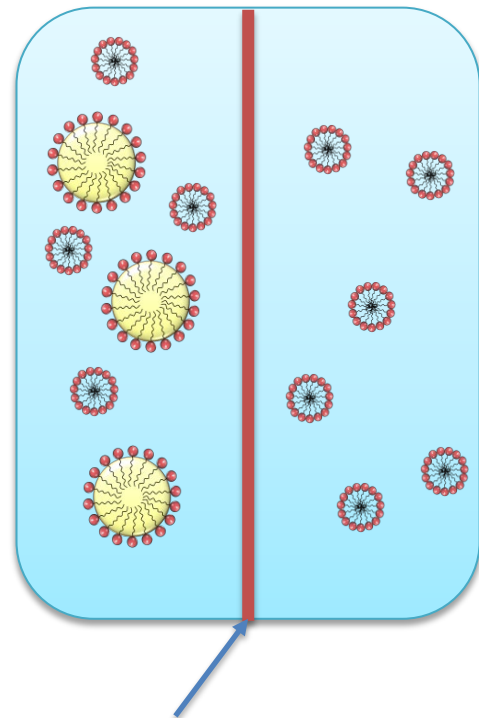
IVRT by (Reverse) Dialysis: A Typical Example



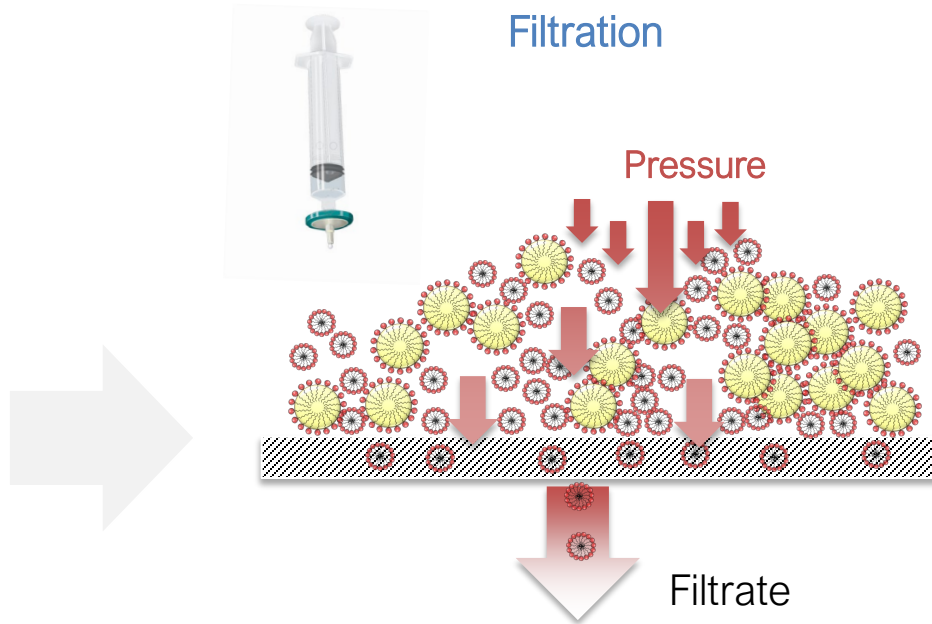
USP 2 with Reverse Dialysis



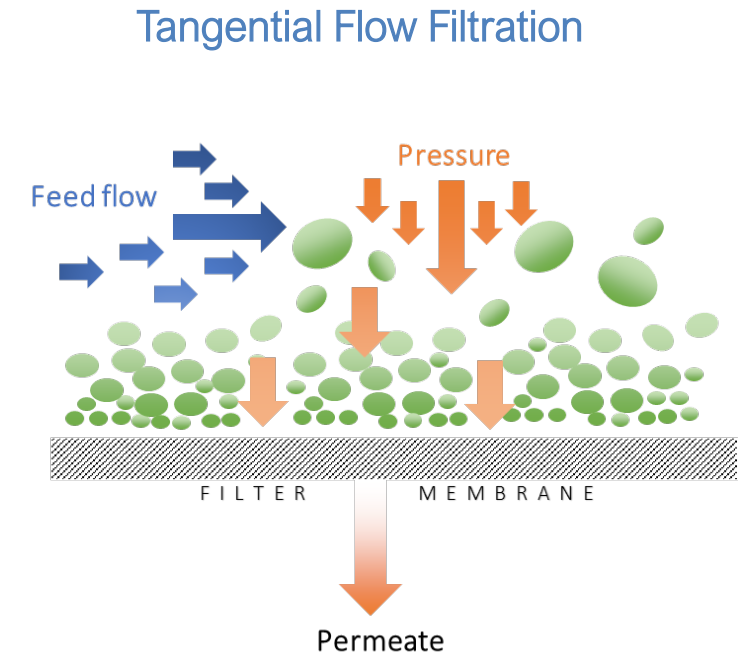
Filtration, Instead of Diffusion



Membrane

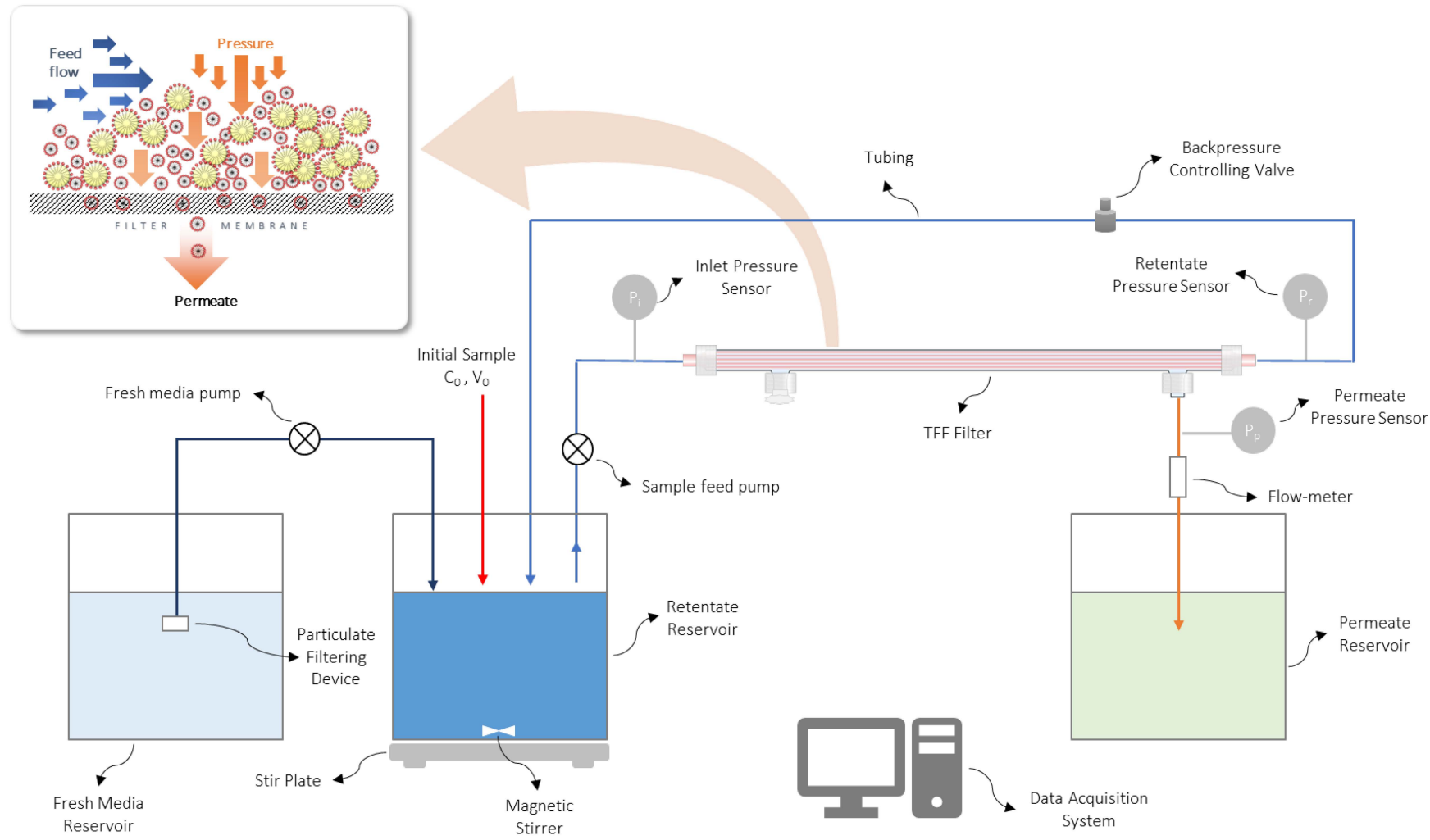


- Pressure driven
- Controllable flow by filtration
- Separation based on membrane size



- Tangential flow, thus avoiding build up at the membrane surface (swept away by flow)

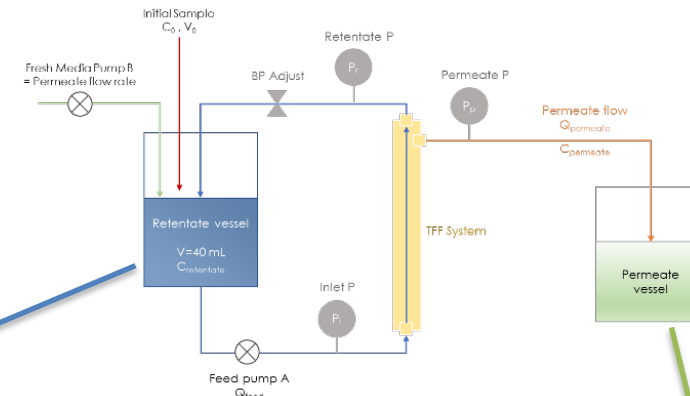
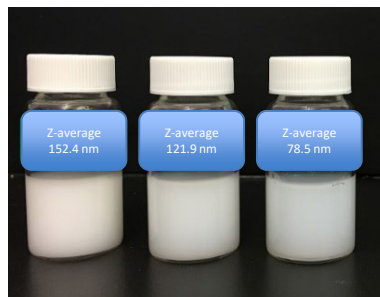
Schematic Diagram of Adaptive Perfusion



Where we started...

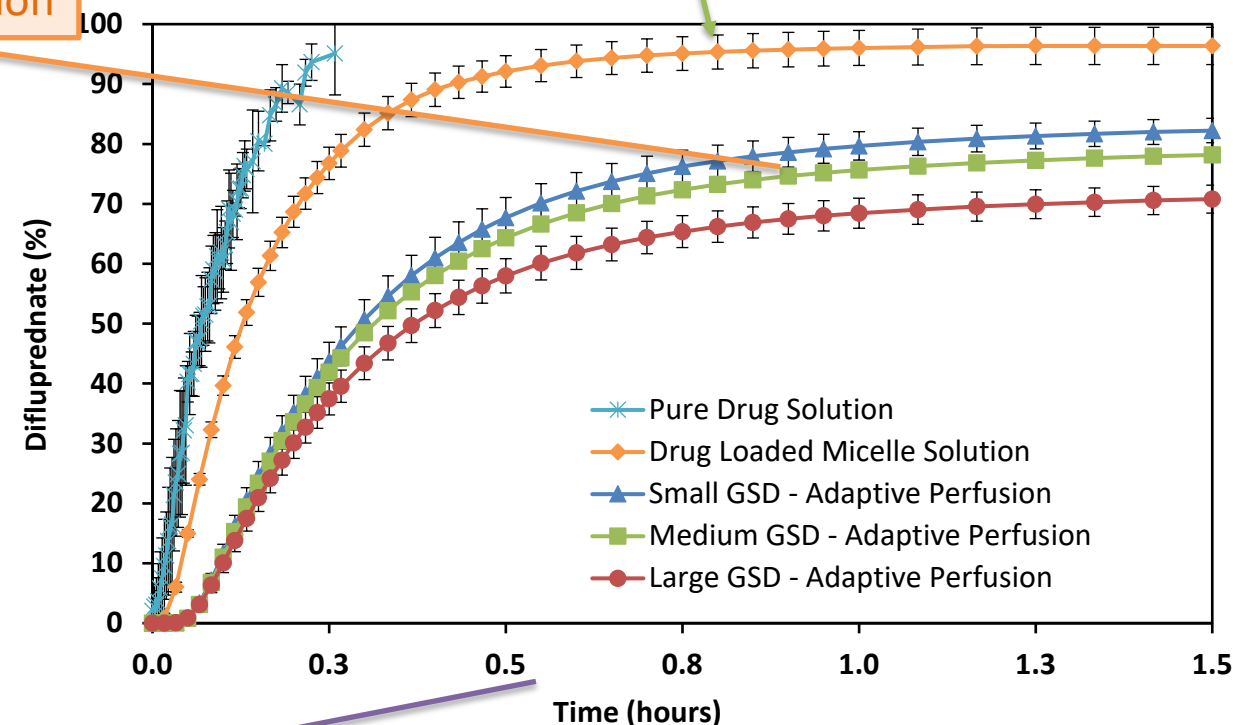
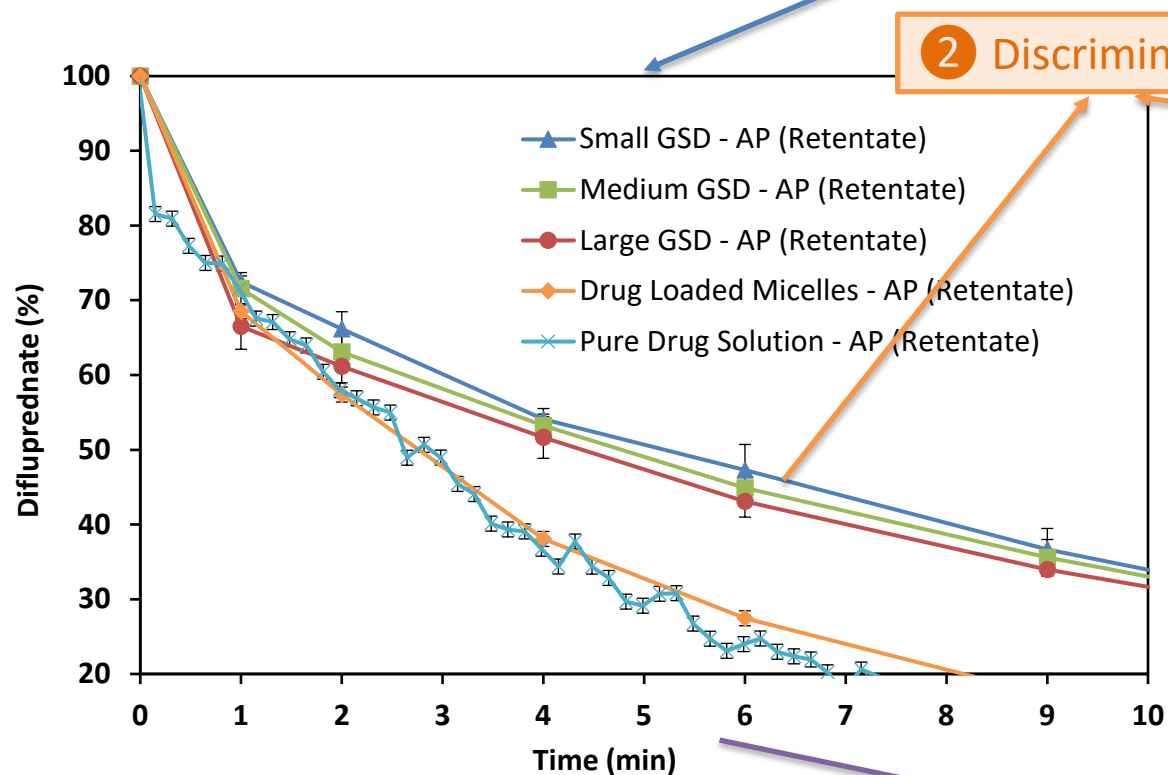


Results



Retentate Concentration Profile (n=3)

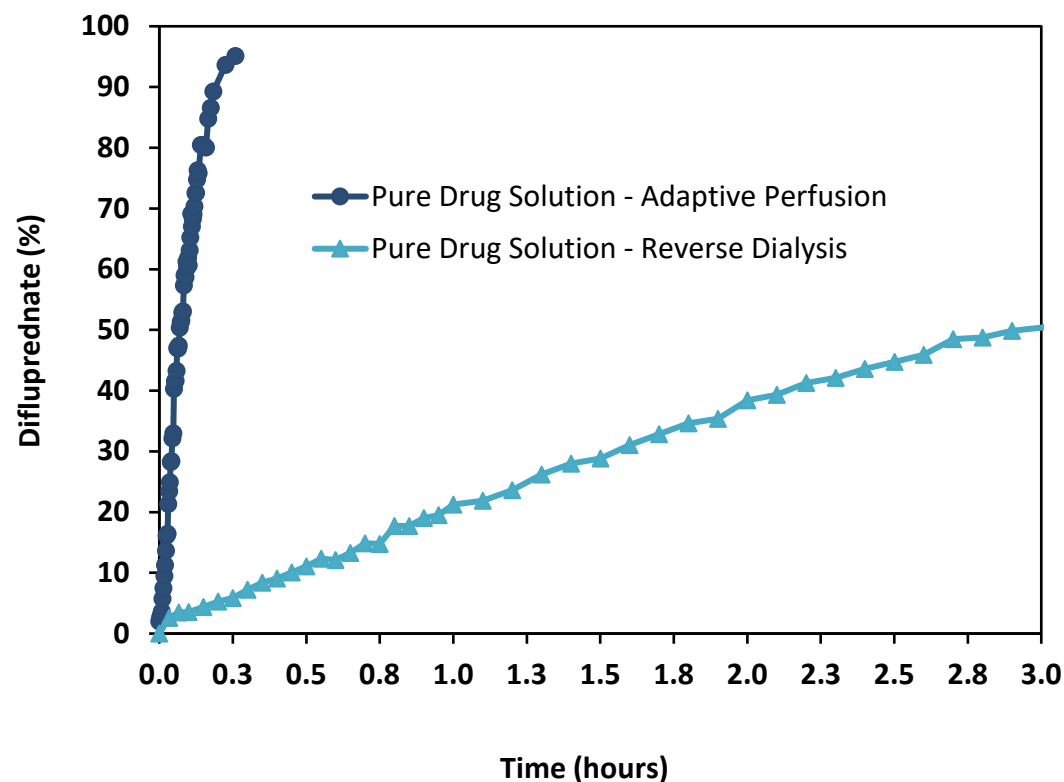
Permeate Concentration Profile (n=3)



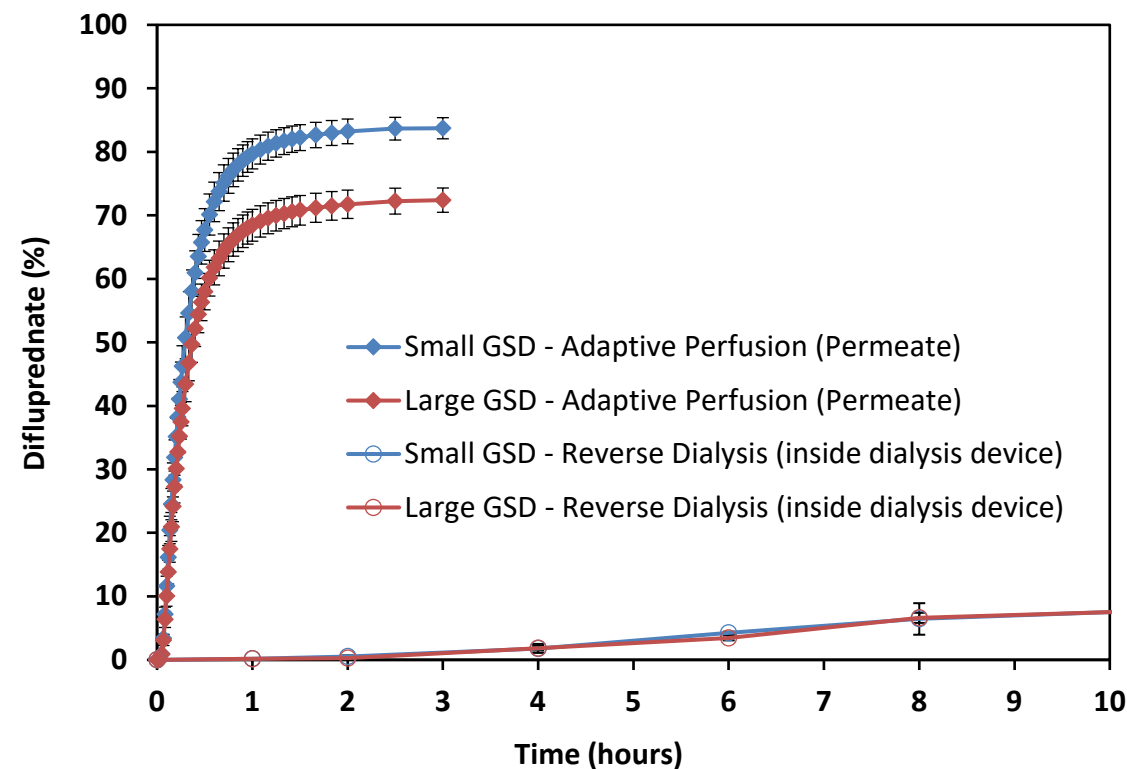
1 Fast

New vs. Old

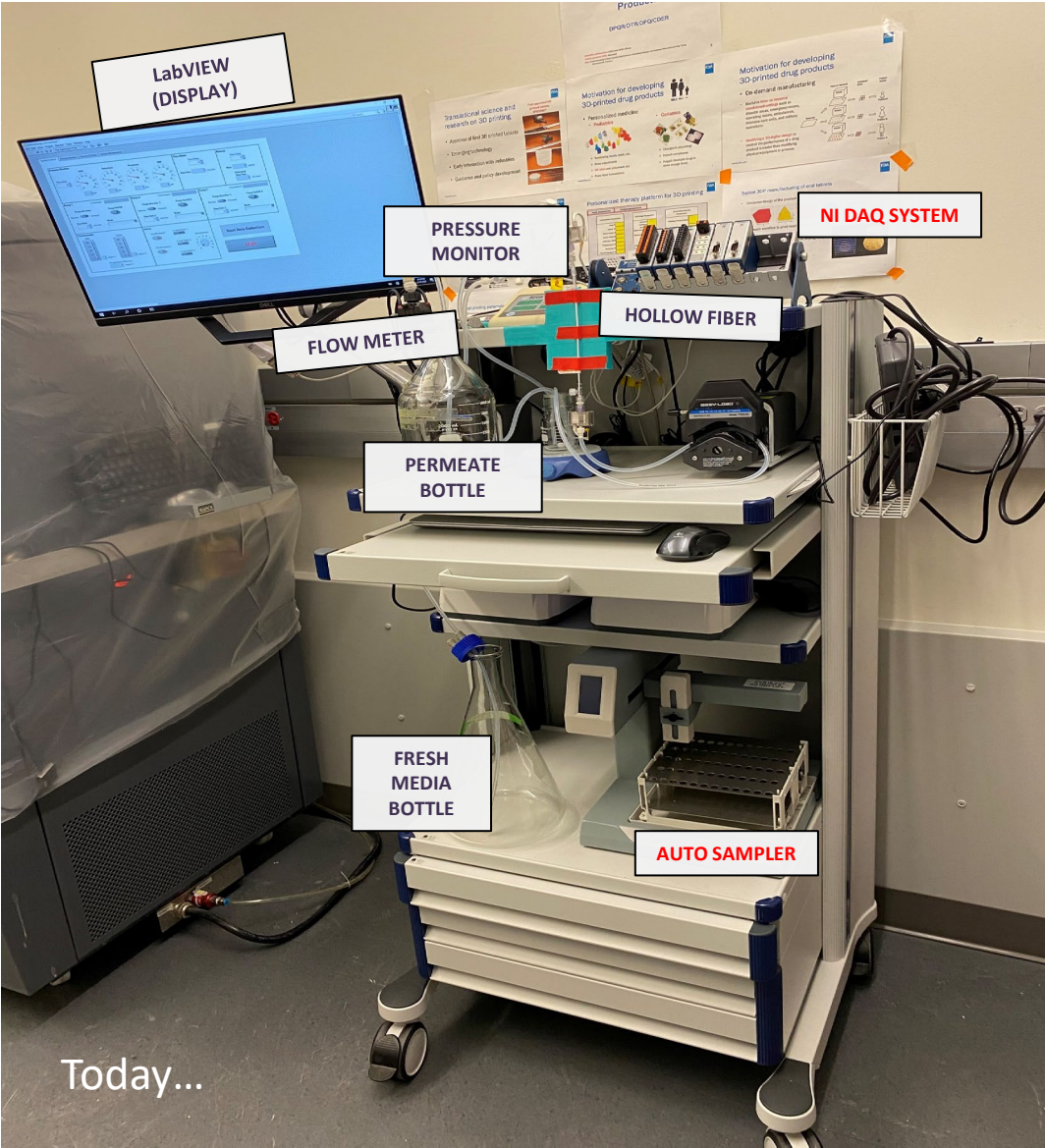
Pure Drug Solution (n = 3)



Small and Large GSD nanoemulsions (n = 3)



Future: A Turnkey Solution



Custom Designed Control Interface

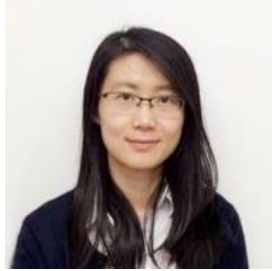
System Startup	Pressure Reading Time Delay: 0 Inlet: 0 psi, Retentate: 0 psi, Permeate: 0 psi, TMP: 0 psi	Flow Meter Reading Time Delay: 0 Flow Rate: 0 mL/min	Backpressure Setting 0 1 2 3 4 5 6 7 8 9 10
Experimental			
Pre-Condition	Valve Control Valve 1: 4-ways switch, Valve 2: 3-ways switch, Valve 3: 3-ways switch, Valve 4: 2-ways switch, Valve 5: 3-ways switch, Valve 6: 3-ways switch		
Run-time			
Re-conditioning	Balance Control Balance 1: Tear, Zero, 0.000 g Balance 2: Tear, Zero, 0.000 g		
Process Monitor	Pump Control and Calibration Pump 1: Initialization: OK, Direction: [Clockwise/Counter-clockwise], Flow rate: 100 mL/min, Tubing size: 16, Calibration: Start Cal. Pump 2: Initialization: OK, Direction: [Clockwise/Counter-clockwise], Flow rate: 5.0 mL/min, Tubing size: 16, Calibration: Start Cal.		

Today...

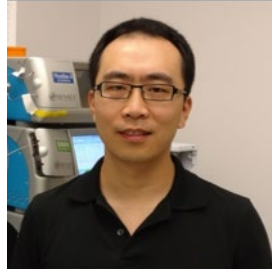
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- Naresh Pavurala
- Darby Kozak
- Stephanie Choi
- Yan Wang
- Jiwen Zheng
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- Bing Cai

Thank you

